## LUNG VOLUMES \& CAPACITIES

## osms.it/lung-volumes-capacities

- Spirometry: spirometer used to measure air volume moving in, out of lungs
- Static lung volumes: volumes not involved in airflow rate
- Capacities: combination of > one lung volume


## Volume variations

- Related to age, sex, body size, posture
- Tidal volume ( $\mathrm{V}_{\mathrm{T}}$ )
- 500 mL
- Air volume inspired, expired during quiet breathing
- Inspiratory reserve volume
- Maximum volume inhaled air above $V_{T}$ = 3L
- Expiratory reserve volume
- Maximum expired air volume below $\mathrm{V}_{\mathrm{T}}$ $=1.2 \mathrm{~L}$
- Residual volume (RV)
- Air remaining in lungs after forced expiration = 1.2L (not measured by spirometry)
- Functional residual capacity (FRC)
- Expiratory reserve volume (ERV) + RV $=2.4 \mathrm{~L}$
- $\mathrm{V} \mathrm{T}+$ inspiratory reserve volume $=3.5 \mathrm{~L}$
- Vital capacity ( $V_{C}$ )
- $\mathrm{V}_{\mathrm{T}}+$ inspiratory reserve volume (IRV) + $E R V=4.7 \mathrm{~L}$
- Total lung capacity (TLC)
- Combination of all lung capacities $=5.9 \mathrm{~L}$


## MEASURING FRC

## Helium dilution method

- Helium placed in spirometer $\rightarrow$ inhaled
- Helium concentration in lungs equalizes with amount of helium placed in spirometer (helium insoluble in blood) after few breaths
- Total helium mass measured in spirometer = FRC


## Body plethysmograph method

- Application of Boyle's law ( $\mathrm{P} \times \mathrm{V}=\mathrm{k}$ )
- Person sits inside plethysmograph (airtight box) $\rightarrow$ breathes in/out through mouthpiece $\rightarrow$ measures air pressure in mouth
- Mouthpiece closed after expiring $V_{T}$; as person attempts to breathe FRC calculated using measurements of alveolar pressure, lung volume, pressure changes within plethysmograph


## ANATOMIC \& PHYSIOLOGIC DEAD SPACE

## osms.it/anatomic-physiologic-dead-space

- Dead space: air volume enters airways, lungs; no gas exchange occurs


## ANATOMIC DEAD SPACE

- Air inaccessible to body for gas exchange (due to anatomical structure)
- Air contained in conducting zone (nose $\rightarrow$ terminal bronchioles)
- Conduit for air movement in/out of lungs; warms, humidifies air; removes debris, pathogens
- Volume $=150 \mathrm{~mL}$ ( $1 / 3$ of tidal volume)


Figure 68.1 The volume of air contained in the conducting zone is called anatomic dead space because no gas exchange occurs here; therefore, no oxygen can be extracted from this air.

## PHYSIOLOGIC DEAD SPACE

- Air physiologically inaccessible to body for gas exchange
- Composition: anatomic dead space + dead space in respiratory zone (respiratory bronchioles, alveolar duct, alveolar sac, alveoli) that does not partake in gas exchange
- Ventilation/perfusion defect: alveoli ventilated, not well perfused (alveolar dead space)
- Volume = approx. 0 (in healthy adult)
- Anatomic dead space = physiologic dead space

$$
V_{T}=V_{D}+V_{A}
$$

- $\mathrm{V}_{\mathrm{T}}$ = tidal volume
- $\mathrm{V}_{\mathrm{D}}=$ physiological dead space volume
- $\mathrm{V}_{\mathrm{A}}$ = air volume present in functioning alveoli


Figure 68.2 The green block represents residual air from the previous inhalation that participated in gas exchange. The purple blocks represent new oxygenated tidal volume inhaled during the current breath. Some of this new air also ends up being dead space air ("alveolar dead space") due to an inadequate blood supply to the alveolus.

## Physiological dead space volume (Bohr equation)

- Assumptions
- Environmental air $\mathrm{CO}_{2}=0$ (actual amount $\cong 0.04 \%$ )
- Dead space $\mathrm{CO}_{2}$ contribution $=0$
- All $\mathrm{CO}_{2}$ in exhaled air comes from functioning alveoli
- $\mathrm{V}_{\mathrm{D}}=\mathrm{V}_{T} \times$ arterial $\mathrm{CO}_{2}$ partial pressure
$\left(\mathrm{PaCO}_{2}\right)$ - expired $\mathrm{CO}_{2}$ partial pressure $\left(\mathrm{PeCO}_{2}\right) \div \mathrm{PaCO}_{2}$

$$
V_{D}=V_{T} \times \frac{P a_{C O_{2}}-P e_{C O_{2}}}{P a_{C O_{2}}}
$$

## VENTILATION

## osms.it/ventilation

- Air movement between environment, lungs
- Ventilation rates: measure air volume moving in/out of lungs over period of time


## MINUTE VENTILATION $\left(V_{E}\right)$

- $V_{E}=$ amount of air moved in/out of lungs in one minute; does not factor in physiological dead space
$\mathrm{V}_{\mathrm{E}}=(\mathrm{VT}) \times($ Respiratory Rate/RR) $\mathrm{V}_{\mathrm{E}}=500 \mathrm{~mL} \times 15 / \mathrm{minute}=7.5 \mathrm{~L} / \mathrm{minute}$


## ALVEOLAR VENTILATION $\left(V_{A}\right)$

- $\mathrm{V}_{\mathrm{A}}=\mathrm{V}_{\mathrm{E}}$ corrected for physiological dead space

$$
V_{A}=(V T-V D) \times R R
$$

$V_{A}=(500 \mathrm{~mL}-150 \mathrm{~mL}) \times 15=5.2 \mathrm{~L} /$ minute

- $V_{A}$ without measuring dead space
- $\mathrm{V}_{\mathrm{A}}=$ volume of $\mathrm{CO}_{2}\left(\mathrm{~V}_{\mathrm{CO} 2}\right) \div$ fraction $\mathrm{CO}_{2}$ ( $\mathrm{F}_{\mathrm{CO}}$ )
$\mathrm{VA}=\left(\mathrm{V}_{\mathrm{co} 2}\right) /\left(\mathrm{F}_{\mathrm{co} 2}\right)$
- Partial pressure: proportional to fractional concentration of that gas in mixture; based on constant K
- Assumes gases are saturated with water vapor (normal body temperature, sea-level atmospheric pressure)
- $\mathrm{CO}_{2}$ partial pressure in alveolar air: $P_{\mathrm{CO} 2}=\mathrm{F}_{\mathrm{CO} 2} \times \mathrm{K}$
- Alveolar ventilation equation: $\mathrm{V}_{\mathrm{A}}=\left[\left(\mathrm{V}_{\mathrm{CO} 2}\right) /\left(\mathrm{P}_{\mathrm{CO} 2}\right)\right] \times \mathrm{K}$
- Replacing $\mathrm{P}_{\mathrm{CO} 2}$ with $\mathrm{co2}$ pressure in arterial blood ( $\mathrm{Pa}_{\mathrm{CO} 2}$ ) in alveolar equation
- Inverse relationship between alveolar ventilation, $\mathrm{CO}_{2}$ partial pressure in alveolar air, pulmonary arteries (e.g. $\uparrow$ air ventilating the alveoli $\rightarrow \downarrow \mathrm{CO}_{2}$ in blood, vice versa)

$$
V_{A}=\frac{V_{C O_{2}} \times K}{P_{A C O_{2}}}
$$

## ALVEOLAR GAS EQUATION

## osms.it/alveolar-gas-equation

- Pressure in alveoli = atmospheric pressure ( $\mathrm{P}_{\text {atm }}$ ); air in alveoli contains water vapor
- Alveolar pressure ( $\mathrm{P}_{\text {atm }}$ ) = water vapor pressure $\left(P_{\text {vapor }}\right)+$ gas mixture pressure $\rightarrow$ total alveolar pressure exerted from all gases minus water vapor $=P_{\text {atm }}-P_{\text {vapor }}$
- $\mathrm{O}_{2}$ partial pressure dissolved in blood ( $\mathrm{P}_{\mathrm{aO} 2}$ ) $=\mathrm{CO}_{2}$ partial pressure in alveoli $\left(\mathrm{P}_{\mathrm{ACO}}\right) \div$ by R (respiratory quotient)

$$
P_{\mathrm{aO2}}=\left(\mathrm{P}_{\mathrm{ACO2}}\right) / R
$$

- Partial pressure of $\mathrm{O}_{2}$ inside alveolus ( $\mathrm{P}_{\mathrm{AO}}$ ) $=$ partial pressure of inspired oxygen $\left(\mathrm{P}_{\mathrm{i} 02}\right)$ minus partial pressure of oxygen going into blood ( $\mathrm{P}_{\mathrm{aO} 2}$ )


## Partial pressure: gas particle mixture

- Gas' partial pressure proportional to fractional gas concentration in mixture
- Fractional $\mathrm{CO}_{2}$ concentration $\left(\mathrm{F}_{\mathrm{CO} 2}\right)=0.3$
- Accounts for $30 \%$ of gas molecules ( $\mathrm{F}_{\mathrm{CO} 2} \times$ total pressure of gas mixture $P_{\text {gases }}$ )
- Fractional concentration of $\mathrm{O}_{2}\left(\mathrm{~F}_{\mathrm{O} 2}\right)=0.7$
- Accounts for remaining 70\% ( $F_{02} \times$ total pressure of gas mixture $P_{\text {gases }}$ )
- Pressure exerted by $\mathrm{O}_{2}>$ pressure exerted by $\mathrm{CO}_{2}$ (proportional to fractional concentrations)
- If $P_{\text {gases }}=20 \mathrm{mmHg}$; partial pressure of $\mathrm{O}_{2}=14 \mathrm{mmHg}(0.7 \times 20)$; partial pressure of $\mathrm{CO}_{2}=6 \mathrm{mmHg}(0.3 \times 20)$
- Partial pressure of inspired air ( $\mathrm{P}_{\mathrm{iO} 2}$ ), fractional oxygen concentration in inspired air ( $\mathrm{F}_{\mathrm{iO} 2}$ ), accounting for water vapor

$$
P_{i 02}=F_{i 02} \times\left(P_{\mathrm{atm}}-P_{\text {vapor }}\right)
$$

## Alveolar gas equation

- Relationship between $\mathrm{O}_{2}$ partial pressure inside alveolus to $\mathrm{CO}_{2}$ partial pressure in alveolus

$$
\begin{gathered}
P_{\mathrm{AO2}}=\left[\mathrm{F}_{\mathrm{iO2}} \times\left(\mathrm{P}_{\mathrm{atm}}-P_{\text {vapor }}\right)\right]-\left[\left(\mathrm{P}_{\mathrm{ACO} 2}\right) / R\right] \\
\mathrm{P}_{\mathrm{AO2}}=150-\left(1.25 \times \mathrm{P}_{\mathrm{ACO} 2}\right) \\
\left.-\mathrm{F}_{\mathrm{iO2}}=0.21 \text { (normal air }=21 \% \mathrm{O}_{2}\right) \\
- \text { Atmospheric pressure }=760 \mathrm{mmHg} \\
- \text { Water vapor pressure } \mathrm{i}=47 \mathrm{mmHg} \\
\mathrm{R}=0.8
\end{gathered}
$$

## COMPLIANCE OF LUNGS \& CHEST WALL

## osms.it/compliance-lungs-chest-wall

- Compliance measures how changes in pressure $\rightarrow$ lung volume change
- Lung, chest wall compliance: inversely correlated with elastic, "snap back" properties (elastance)
- Compliance $=\Delta V / \Delta P$
- Elastance $=\triangle \mathrm{P} / \Delta \mathrm{V}$
- $\uparrow$ compliance $\rightarrow$ lungs easier to fill with air
- Forces promoting open alveoli: compliance, transmural pressure gradient, surfactant
- $\downarrow$ compliance $\rightarrow$ lungs harder to fill with air
- Forces promoting collapse of alveoli: elastic recoil/elastance, alveolar surface tension


## COMBINED PRESSURE-VOLUME CURVES FOR THE LUNG \& CHEST WALL

## osms.it/pressure-vol_curves_lung_chest_wall

- Pressure-volume relationship is curvilinear
- Volume at FRC (zero airway pressure)
- Lung inward recoil: balanced with chest wall's tendency to expand outward (e.g. at equilibrium with no tendency to collapse/expand)
- Volume > FRC
- Positive transmural pressure
- $\uparrow$ lung recoiling force
- $\downarrow$ chest wall outward force
- Volume < FRC (forced expiration)
- Negative transmural pressure
- $\downarrow$ lung recoiling force
- $\uparrow$ chest wall outward force
- Pressure-volume curves plotted on graph
- X-axis: pressure
- Y axis: volume
- Slope of curve = compliance
- Curve flattens out when lung, chest wall compliance combined
- Hysteresis: compliance for inspiration, expiration are different $\rightarrow$ slopes will be different


## ALVEOLAR SURFACE TENSION \& SURFACTANT

## osms.it/alveolar-surface-tension-surfactant

- Alveoli lined with fluid film; water tends to form spheres (e.g. drops)
- Due to intrinsic surface tension (caused by attraction of water molecules to each other)
- Surface tension creates pressure $\rightarrow$ pulls alveoli closed $\rightarrow$ collapses into sphere $\rightarrow \downarrow$ gas exchange
- Law of Laplace: pressure that promotes lungs' collapse is (1) directly proportional to surface tension, (2) inversely proportional to alveoli radius

$$
P=2 T / r
$$

- $\mathrm{P}=$ pressure on alveolus
- $T=$ surface tension
- r = alveolar radius
- Smaller alveolus $(r=1) \rightarrow \uparrow$ pressure - $P=2 \times 50 / 1=100$
- Larger alveolus $(r=2) \rightarrow \downarrow$ pressure - $P=2 \times 50 / 2=50$
- Alveoli are small (allows $\uparrow$ surface area relative to volume), so have $\uparrow$ collapsing pressure


## SURFACTANT

- $\downarrow$ collapsing pressure in alveoli $\rightarrow \uparrow$ gas exchange, $\uparrow$ lung compliance, $\downarrow$ work of breathing
- Lipoprotein mixture primarily containing dipalmitoyl phosphatidylcholine (DPPC)
- Synthesized by type II pneumocytes, coats inside of alveoli
- Contains both hydrophilic, hydrophobic group (amphipathic nature) -
repelling hydrophobic groups, attracting intermolecular forces produced by hydrophilic groups $\rightarrow \downarrow$ surface tension, collapsing pressure


## AIRFLOW, PRESSURE, \& RESISTANCE

## osms.it/airflow-pressure-resistance

## AIR FLOW \& PRESSURE

- Airflow in lungs determined by Ohm's law
- Air flow directly proportional to pressure difference between alveoli, mouth/ nose; inversely proportional to airway resistance

$$
\mathrm{Q}=\Delta \mathrm{P} / \mathrm{R}
$$

- $Q=$ air flow
- $\Delta P=$ change in pressure
- $R=$ resistance
- Pressure gradient
- Driving force for air flow
- Diaphragm contracts during inspiration
$\rightarrow$ creates pressure gradient ( $\uparrow$ lung volume, $\downarrow$ alveolar pressure) $\rightarrow$ air flows into lungs


## RESISTANCE

## Poiseuille's law

- Resistance in lungs determined by Poiseuille's law
- Air flow directly proportional to resistance along airway

$$
R=\frac{8 n l}{\pi r^{4}}
$$

- $R=$ resistance
- $\mathrm{n}=$ gas viscosity
- I = length of airway
- $\boldsymbol{\pi r} 4=$ flow is related exponentially to airway's radius
- Highlights critical importance of airway diameter on airflow
- E.g. if airway radius $\downarrow$ by a factor of $2 \rightarrow$ $\uparrow$ resistance by 24 (16-fold)


## Resistance changes

- Parasympathetic muscarinic receptor stimulation $\rightarrow$ bronchial smooth muscle constriction $\rightarrow \downarrow$ airway diameter $\rightarrow \downarrow$ airflow; sympathetic stimulation of $\beta 2$ receptors $\rightarrow$ bronchial smooth muscle relaxation $\rightarrow \uparrow$ airway diameter $\rightarrow \uparrow$ airflow
- $\downarrow$ lung volume $\rightarrow \uparrow$ resistance; $\uparrow$ lung volume $\rightarrow \downarrow$ resistance
- $\uparrow$ viscosity (e.g. deep sea diving) $\rightarrow \uparrow$ resistance; $\downarrow$ viscosity (e.g. inhaling helium) $\rightarrow \downarrow$ resistance


## BREATHING CYCLE

## osms.it/breathing-cycle

- Normal, quiet breathing phases
- Rest (period between breaths), inspiration, expiration
- Involves changes in air volume, intrapleural pressure, alveolar pressure
- Affected by respiratory system's resistance, compliance


## Rest

- Alveolar pressure $\left(\mathrm{P}_{\text {alv }}\right)=$ atmospheric pressure $\left(P_{\text {atm }}\right)=0$
- No air movement in/out of lungs
- Due to pressure gradient's absence
- Air volume in lungs = FRV
- Intrapleural pressure $=-0.5 \mathrm{cm0} 0.2 \mathrm{in} \mathrm{H}_{2} \mathrm{O}$
- Transmural pressure gradient (intrapleural pressure always less than alveolar pressure) keeps lungs inflated
- Diaphragm relaxed

Inspiration

- Active process (requires muscle activity)
- Diaphragm (major inspiratory muscle; innervated by phrenic nerve) contracts, moves downward; external intercostal
muscles contract (innervated by intercostal nerves) contract, elevate ribs outward, upward $\rightarrow$ enlarge thoracic cavity $\rightarrow \uparrow$ lung volume $\rightarrow \downarrow$ pressure in lungs ( $\mathrm{P}_{\mathrm{alv}}=$ $-1 \mathrm{~cm} / 0.39$ in $\mathrm{H}_{2} \mathrm{O}$ )
- Boyle's law ( $P=k / V$ ): gas pressure ( $P$ ) in container (thorax, alveoli) at constant temperature (k) inversely proportional to volume (V)
- Pressure gradient causes air to flow into lungs until $P_{\text {alv }}=P_{\text {atm }}$ at inspiration's end
- Volume in lungs = FRC + VT
- Intrapleural pressure $=-8 \mathrm{~cm} / 3.1$ in $\mathrm{H}_{2} \mathrm{O}$ at expiration's end


## Expiration

- Passive process
- Elastic forces of lungs compress alveolar air volume $\rightarrow \uparrow$ pressure in lungs $\rightarrow P_{\text {alv }}>P_{\text {atm }}$ $\rightarrow$ pressure gradient causes air to flow out of lungs until $P_{\text {alv }}=P_{a t m}$ at inspiration's end
- Diaphragm, external intercostal muscles relax $\rightarrow \downarrow$ thoracic cavity size $\rightarrow \downarrow$ lung volume $\rightarrow \uparrow$ pressure in lungs
- $V_{T}$ expired $\rightarrow$ lung volume $=F R C$

